

Research



Cite this article: Tang Y, Wu J, Zhang Y, Ju L, Qu X, Jiang D. 2021 Magnetic transfection with superparamagnetic chitosan-loaded IGFBP₅ nanoparticles and their *in vitro* biosafety. *R. Soc. Open Sci.* **8**: 201331.
<https://doi.org/10.1098/rsos.201331>

Received: 15 August 2020

Accepted: 24 November 2020

Subject Category:

Chemistry

Subject Areas:

nanotechnology

Keywords:

osteosarcoma, IGFBP₅, biosafety, superparamagnetic chitosan iron oxide nanoparticles, magnetic transfection

Authors for correspondence:

Xiangyang Qu

e-mail: drqxy04090@126.com

Dianming Jiang

e-mail: 201296@hospital.cqmu.edu.cn

This article has been edited by the Royal Society of Chemistry, including the commissioning, peer review process and editorial aspects up to the point of acceptance.



Magnetic transfection with superparamagnetic chitosan-loaded IGFBP₅ nanoparticles and their *in vitro* biosafety

Yue Tang^{1,2,3}, Jun Wu², Yuan Zhang², Lingpeng Ju², Xiangyang Qu² and Dianming Jiang^{1,3}

¹Department of Traumatic Joint Center, The Third Affiliated Hospital of Chongqing Medical University (General Hospital), No 1 Shuanghu Road, Yubei District, Chongqing 401120, People's Republic of China

²Department of Orthopedics, Children's Hospital of Chongqing Medical University, National Clinical Research Center for Child Health and Disorders, Ministry of Education Key Laboratory of Child Development and Disorders, Chongqing Key Laboratory of Pediatrics, Laboratory of Biomaterials, 136# Zhongshan 2 road, Yuzhong District, Chongqing 400014, People's Republic of China

³Department of Orthopedics, The First Affiliated Hospital of Chongqing Medical University, No 1 Medicine Road, Yuzhong District, Chongqing 400016, People's Republic of China

YT, 0000-0003-1470-3877; DJ, 0000-0001-9935-7066

We prepared the superparamagnetic chitosan nanoparticles (SPCIONPs) to study the application of them as gene vectors using a magnetic transfection system for the targeted treatment of lung metastasis of osteosarcoma. The SPCIONPs were characterized by transmission electron microscopy, Fourier transform infrared spectrometry, superconducting quantum interference device and atomic force microscopy. Their biosafety was determined by cell counting kit-8 (CCK8) and live–dead staining assays. The transfection *in vitro* was detected by laser confocal microscopy. SPCIONPs, which can bind closely to plasmids and protect them from DNA enzyme degradation, were prepared with an average particle size of approximately 22 nm and zeta potential of 11.3 mV. The results of the CCK8 and live–dead staining assays showed that superparamagnetic chitosan nanoparticles loaded with insulin-like growth factor-binding protein 5 (SPCIONPs/pIGFBP₅) induced no significant cytotoxicity compared to the control group. The result of transfection *in vitro* suggested that pIGFBP₅ emitted a greater amount of red fluorescence in the SPCIONPs/pIGFBP₅ group than that in the chitosan-loaded IGFBP₅ (CS/pIGFBP₅) group. In conclusion, the prepared SPCIONPs had good biosafety and could be effectively used to transfer pIGFBP₅ into 143B cells, and they thus have good application prospects for the treatment of lung metastasis of osteosarcoma.

1. Introduction

Osteosarcoma is the most common primary bone malignancy in children and young people, with lung metastases occurring at the time of diagnosis in approximately 15–20% of patients [1]. At present, a multimodal treatment approach has been adopted for osteosarcoma treatment, with a methotrexate, doxorubicin and cisplatin (MAP) regimen as the first choice. The treatment is mainly based on chemotherapy combined with limb salvage or amputation, but the clinical therapeutic effect is still unsatisfactory. The 5-year survival rate for patients with osteosarcoma is approximately 70%, while the survival rate for patients with metastatic or recurrent disease is extremely low, with an overall survival rate of less than 20% [2]. Therefore, gene therapy has become a trend in osteosarcoma treatment [3].

Insulin-like growth factor-binding protein 5 (IGFBP₅) is a member of the insulin-like growth factor (IGF) system, which plays an important role in cell growth, differentiation and apoptosis [4]. IGFBP₅ primarily binds to insulin growth factors to inhibit the IGF1 and IGF2 signalling pathways, thereby inhibiting the proliferation, migration and invasion of osteosarcoma, and is a key inhibitor of *in situ* osteosarcoma growth and lung metastasis [5]. Our group previously used adenovirus to induce IGFBP₅ overexpression in osteosarcoma cells and confirmed that IGFBP₅ can induce apoptosis and inhibit invasion, migration and proliferation of osteosarcoma cells [6].

Non-viral gene vectors, which are currently a focus of research, will not cause immune responses, potential immunogenicity and lethal inflammation, in contrast to adenovirus vectors [7,8]. Non-viral vectors commonly include liposomes, polyethyleneimine (PEI) and chitosan (CS). Cationic liposomes, which have higher transfection rates but are more toxic and expensive, are the most commonly used liposomes. Cationic liposomes also have no sustained-release effect and thus require repeated administration during experiments *in vivo*, and they are greatly affected by serum [9]. PEI is currently the most commonly used and most effective non-viral vector due to its strong proton-buffering capacity. PEI is the gold standard for polymeric gene delivery vectors. The proton sponge effect can cause endosomes to swell and release the plasmid into the cytoplasm, which allows the plasmid to enter the nucleus and complete gene expression [10,11]. Therefore, PEI was used as a positive control group in this study. However, due to its severe toxicity, including mitochondrial damage and apoptosis, the *in vivo* applications of PEI are limited [12,13]. CS is currently used in tissue engineering, drug and gene delivery, wound healing, and antibacterial and anti-tumour applications because of its physiological and biological activity; biocompatibility with a variety of organs, tissues and cells; low toxicity, with generally recognized as safe (GRAS) approval by the Food and Drug Administration (FDA) [14–16] and compatibility with chemical or enzymatic modifications. In addition, CS can be dissolved in acetic acid to condense the plasmid and prevent degradation by DNase, and it is a good substitute for viral vectors, but unmodified CS has a low transfection rate as a gene vector [17].

Superparamagnetic iron oxide nanoparticles (SPIONPs) can act as a reagent with both active and passive targeting effects and can concentrate the carried drugs in the target tissue under the effect of an external magnetic field. Because of their advantages, such as biocompatibility, stability, environmental safety and low price, SPIONPs are widely used in biomedicine, including for targeted drug delivery [18–21], bioimaging, thermotherapy, photoablation therapy, biosensing and thermal olfaction [22–25]. At present, there are many studies to modify the surface of SPIONPs so that its surface is distributed in different groups, such as polymers, biomolecules, silica and metals which can provide the ensemble functional reactive group, e.g. aldehyde groups, hydroxyl groups, carboxyl groups and amino groups. Their groups can be linked to antibodies, proteins, DNA, enzymes and other bioactive substances for further application [26]. Therefore, in this study, we prepared SPIONPs coated with CS to generate superparamagnetic chitosan-coated iron oxide nanoparticles (SPCIONPs) and conducted experimental studies to investigate their *in vitro* biosafety and use for cell transfection in the presence of magnetic transfection system.

2. Material and methods

2.1. Materials

Citric acid, ferric chloride hexahydrate, ferrous sulfate heptahydrate, 25–28 wt% ammonia solution and 1-(3-dimethylaminopropyl)-3-ethylcarbodiimide hydrochloride (EDC) were purchased from Macleans (Shanghai, China); Dulbecco's Modified Eagle Medium (DMEM) and trypsin were purchased from Gibco (CA, USA); chitosan (50 kDa, 98% polyacetyl), *n*-hydroxysuccinimide (NHS) and fluorescein

isothiocyanate (FITC) were purchased from Sigma-Aldrich (MO, USA); fetal bovine serum was purchased from PAN-Biotech (Adenbach, Germany); the Prussian blue staining kit was purchased from Solarbio (Shanghai, China); the DNA marker was purchased from Tiangen (Beijing, China); Hoechst, DNase 1 and LB broth were purchased from Beyotime Biotech (Beijing, China); and the Endo-free Plasmid Maxi Kit-25 was purchased from OMEGA (GA, USA).

2.2. Preparation of SPCIONPs

Ferric chloride hexahydrate (2 g) and ferrous sulfate heptahydrate (1.4 g) were dissolved in 5 ml of water, followed by ultrasonication until the chemicals were completely dissolved. The solution was then transferred to a three-necked flask and stirred under nitrogen. Subsequently, 20 ml of 0.1% citric acid solution was added to the solution, which was then stirred for 10 min. The three-necked flask was then placed in a water bath at 85°C. A total of 20 ml ammonium hydroxide was added with a dropping funnel; the addition was completed within 10 min, and stirring was continued for another 30 min [27,28]. The resulting suspension was centrifuged at 8500 r.p.m. for 10 min, the sediment was discarded, and the supernatant was removed to obtain the ferrofluid of citric acid-coated magnetite particles (SPIONPs). Finally, 5 ml of the ferrofluid of citric acid-coated magnetite particles was added to MES buffer solution with a pH of 5, and EDC and NHS were subsequently added under stirring to activate the carboxyl group on the surface of the ferrofluid of citric acid-coated magnetite particles, followed by the addition of 5 ml of 20 mg ml⁻¹ 50 kDa CS solution in acetic acid and stirring at 300 r.p.m. at room temperature for 6 h [29]. The liquid was collected after 48 h of dialysis with a dialysis bag (retained molecular weight over 50 000). A portion of the liquid was lyophilized and stored at 4°C for later use.

2.3. Characterization

The size and morphology of the prepared SPCIONPs were observed with a transmission electron microscope (TEM, HITACHI, USA). The size distribution was determined by measuring diameters of 100 NPs randomly selected on the TEM micrographs. A Zetasizer Nano ZS (Malvern, UK) was used to determine the zeta potential of the CS, SPIONPs, SPCIONPs and SPCIONPs/pIGFBP₅. The magnetic induction of SPIONPs and SPCIONPs was measured at 300 K using a superconducting quantum interference device (SQUID, a magnetic property measurement system (MPMS), Quantum Design, USA). The structural characterization of CS, SPIONPs and SPCIONPs was performed with a Fourier transform infrared (FT-IR) spectrometer using the KBr compression method. The molecular structure of prepared SPCIONPs were loaded onto the XY scanner of the AFM (IPC-208B, Chongqing University, China) [30–32]; the area to be scanned was localized on the monitor, and then images generated at room temperature under ambient conditions using the non-contact mode. A 100 mm scanner and a STM probe were used in the study, with a customized tungsten filament as the micro-cantilever to detect an area of 12.01 × 12.01 nm.

2.4. Agarose gel electrophoresis

Agarose gel electrophoresis was used to detect the ability of SPCIONPs to condense the plasmids. The SPCIONPs and plasmids (1 µg) were mixed based on N/P ratios of 10/1, 5/1, 2.5/1, 2/1, 1/1, 1/2, 1/2.5, 1/5 and 1/10. A 0.8% agarose gel was prepared with 1% Tris-acetate-EDTA (TAE) buffer, and the samples were electrophoresed at 85 mV for 30 min. The optimal N/P ratios of SPCIONPs and pIGFBP₅ were observed. The naked plasmid was used as the control.

2.5. Protection assay

After incubation of SPCIONPs with the plasmids at different N/P ratios, 1 µl of DNase I (corresponding to 1 µg of plasmid) was added to 10× reaction buffer [100 mM Tris-HCl (pH = 7.5 at 25 mM), 25 mM MgCl₂, 1 mM CaCl₂]. After 15 min of incubation in a 37°C water bath, 1 µl of ethylenediaminetetraacetic acid (EDTA) (25 mM, pH = 8) was added, followed by incubation at 65°C for 15 min to inactivate DNase I. The naked plasmid was used as the control. A 0.8% agarose gel was prepared with 1% TAE, and the samples were electrophoresed at 85 mV for 30 min.

2.6. Prussian blue staining

Prussian blue can stain iron atoms in cells. First, 143B cells were seeded in 12-well plates at 1×10^5 cells/well. After the cells became adherent, SPCIONPs/pIGFBP₅ were added, and a magnetic field was applied for 30 min. After 4 h, the cells were washed three times with phosphate-buffered saline (PBS) and fixed in paraformaldehyde for 20 min. Perls solution was prepared at a 1 : 1 ratio, and 200 μ l of the solution was added to each well, followed by incubation at 37°C for 40 min. Cells were washed with ddH₂O, and 200 μ l of neutral red solution was added and incubated with the cells at room temperature for 2 min. After the staining solution was rinsed with ddH₂O, the cells were observed under a light microscope.

2.7. *In vitro* toxicity assay

The CCK8 reagent was used to calculate the cell survival rate in order to detect cytotoxicity. First, 143B cells were seeded in 96-well plates at 4×10^3 cells/well with five duplicated wells in each group. After the cells became adherent, the reagents were added to each of the following groups: the control group, the PUC19 group (the PUC19 plasmid was used to clone *Escherichia coli* without the target gene), the CS/PUC19 group, the SPCIONPs/PUC19 group and the PEI/PUC19 group, and a magnetic field was applied for 30 min. A total of 10 μ l CCK8 reagent was added at 24 and 48 h, followed by incubation at 37°C for 3 h. The optical density (OD) at 450 nm was detected using a microplate reader, and the cell survival rate was calculated as follows: cell survival rate = (experimental group – blank group) / (control group – blank group) * 100%.

2.8. Live–dead staining

The 143B cells were seeded in a 24-well plate at 5×10^4 cells/well. After the cells became adherent, reagents were added to each of the following groups: the control group, the PUC19 group, the CS/PUC19 group, the SPCIONPs/PUC19 group and the PEI/PUC19 group. The magnetic field was applied for 30 min. The cells were collected by centrifugation and resuspended in a mixture of 1 μ l A (1 mM Live-Dye) + 1 μ l B (1 mg ml⁻¹ PI) + 1 ml staining buffer at 24 h and 48 h. After incubation at 37°C for 15 min in the dark, the cells were observed under a fluorescence microscope. The following method was used to calculate the cell survival rate: number of red cells / (number of red cells + number of green cells) * 100%.

2.9. Cell uptake

The 143B cells were seeded in a 34 mm confocal dish at 1×10^5 cells/well, and FITC-CS/pIGFBP₅ and FITC-SPCIONPs/pIGFBP₅ were added after the cells became adherent. pIGFBP₅ is an expression plasmid with red fluorescence protein (RFP). After a magnetic field was applied for 30 min, the non-endocytosed particles were washed away with PBS, and cell culture was continued for 6 or 24 h. At each time point, the cells were washed with PBS and stained with Hoechst for 20 min. After washing with PBS, the medium was added, and the cells were observed under a confocal microscope.

2.10. *In vitro* transfection assay

The 143B cells were seeded in a 12-well plate, and when the confluency of cells reached 80–90%, the medium was aspirated, and the cells were washed three times with PBS. A total of 800 μ l of supplement-free medium was added to each well, and 4 nM HCl was used to prepare serum-free medium at a pH of 5.5. The CS/pIGFBP₅ and SPCIONPs/pIGFBP₅ was used serum-free medium to dilute to 200 μ l per well, and the mixtures were incubated at 50°C for 20 min and used to transfect cells; 200 μ l PEI was added to the PEI group (positive control group), and a magnetic field was applied for 30 min. After 4 h of transfection, the cells were washed three times with PBS, cultured for 24 h, and observed under an inverted fluorescence microscope.

2.11. Statistical analysis

All analyses were performed using IBM SPSS 20.0 (software version 20.0, SPSS Inc., Chicago, IL, USA) or GraphPad Prism (version 7.00, GraphPad Software, Inc., San Diego, CA, USA). Multigroup comparisons were performed using ANOVA. A value of $p < 0.05$ was considered statistically significant.

3. Results

3.1. Characterization

SPCIONPs were successfully prepared by the dehydration condensation method, and their physico-chemical characterizations were shown in figure 1. The morphology of SPCIONPs was observed by TEM, and the average particle size of a single particle was about 22 nm (figure 1*a,b*). Figure 1*c* shows that the zeta potentials of CS, SPIONPs and SPCIONPs were 42.9, -27.9 and 27.1 mV, respectively. The negatively charged plasmids were combined through electrostatic adsorption to form SPCIONPs/pIGFBP₅, which were positively charged with a zeta potential of 11.3 mV.

A comparison of transverse magnetic induction results (figure 1*d*) indicated that the superparamagnetic behaviour of SPCIONPs was weaker than that of SPIONPs. Both curves intersected the origin, and the hysteresis was zero. Therefore, both were superparamagnetic, which was consistent with previous research results [29,33].

The infrared spectra of CS, SPIONPs and SPCIONPs in the wavenumber range of 400–4000 cm^{-1} are shown in figure 1*e*. The CS spectrum had unique amino (NH_2) characteristic peaks at 3343.63 and 1617.23 cm^{-1} . The spectra of SPIONPs had characteristic COOH peaks, with C=O at 1646.05 cm^{-1} and O–H at 3426.82 cm^{-1} , the characteristic peaks of Fe_3O_4 and Fe–O were observed at 569.91 cm^{-1} . SPCIONPs exhibit the amide bond (NH–CO) formed by the amino group of chitosan and the carboxyl group of SPIONPs, and the characteristic peaks of N–H (3439.63 cm^{-1} and 1617.23 cm^{-1}), C=O (1687.69 cm^{-1}) and Fe–O (579.36 cm^{-1}) were not affected (figure 1*e*).

AFM also verified that CS was bound to SPIONPs by amide bonds. White dots formed a six-membered ring representing the basic structure of CS; black dots represented Fe atoms; and red and white dots bound together represented N–H and C=O (figure 1*f*).

3.2. Plasmid binding assay

After the addition of samples at N/P ratios of 10/1, 5/1, 2.5/1, 2/1, 1/1, 1/2, 1/2.5, 1/5 and 1/10, we found that when the N/P was 2/1, the plasmids did not run out of the electrophoresis lanes, which confirmed that SPCIONPs could fully bind to the plasmids and that the transfection ratio should be greater than or equal to 2/1 (figure 2*a*).

The enzyme protection assay showed that the naked plasmid was completely degraded by DNase I. Moreover, at an $\text{N/P} \geq 2$ and after DNase I addition, the plasmid was not degraded and still gathered in the hole. Figure 2*b* shows that SPCIONPs also protected the plasmids from degradation by DNase.

3.3. Prussian blue assay

Figure 3 shows Prussian blue staining after 4 h of incubation with SPCIONPs/pIGFBP₅. In the SPCIONPs/pIGFBP₅ group, most of the blue particles were concentrated on the cell membrane, and a small number of blue particles were visible in the cells. No significant difference in cell morphology was observed compared to the control group, indicating that SPCIONPs had no obvious cytotoxicity within 4 h.

3.4. CCK8 assay

A CCK8 assay was used to detect the toxicity of PUC19, CS/PUC19, SPCIONPs/PUC19, and PEI/PUC19. Figure 4 shows that the growth of the cells in the PUC19, CS/PUC19, and SPCIONPs/PUC19 groups at 24 h was not inhibited compared to the control group, and the cell survival rate in the SPCIONPs/PUC19 group was even greater than that in the control group, but the difference was not statistically significant. The cell survival rate in the PEI/PUC19 group was $86.59 \pm 0.05\%$, which was significantly different from that in the SPCIONPs/PUC19 group.

After 48 h of the incubation with PUC19, CS/PUC19 or SPCIONPs/PUC19, the cell survival rate was not significantly different from that in the control group, whereas the cell survival rate in the PEI/PUC19 group was $73.37 \pm 0.06\%$, which was also significantly different from that in the SPCIONPs/PUC19 group. No significant difference was observed between the CS/PUC19 and SPCIONPs/PUC19 groups at 24 or 48 h. The overall trend of the live–dead staining assay was generally consistent with that observed in the CCK8 assay. As shown in figure 5, red fluorescence represented dead cells, and green

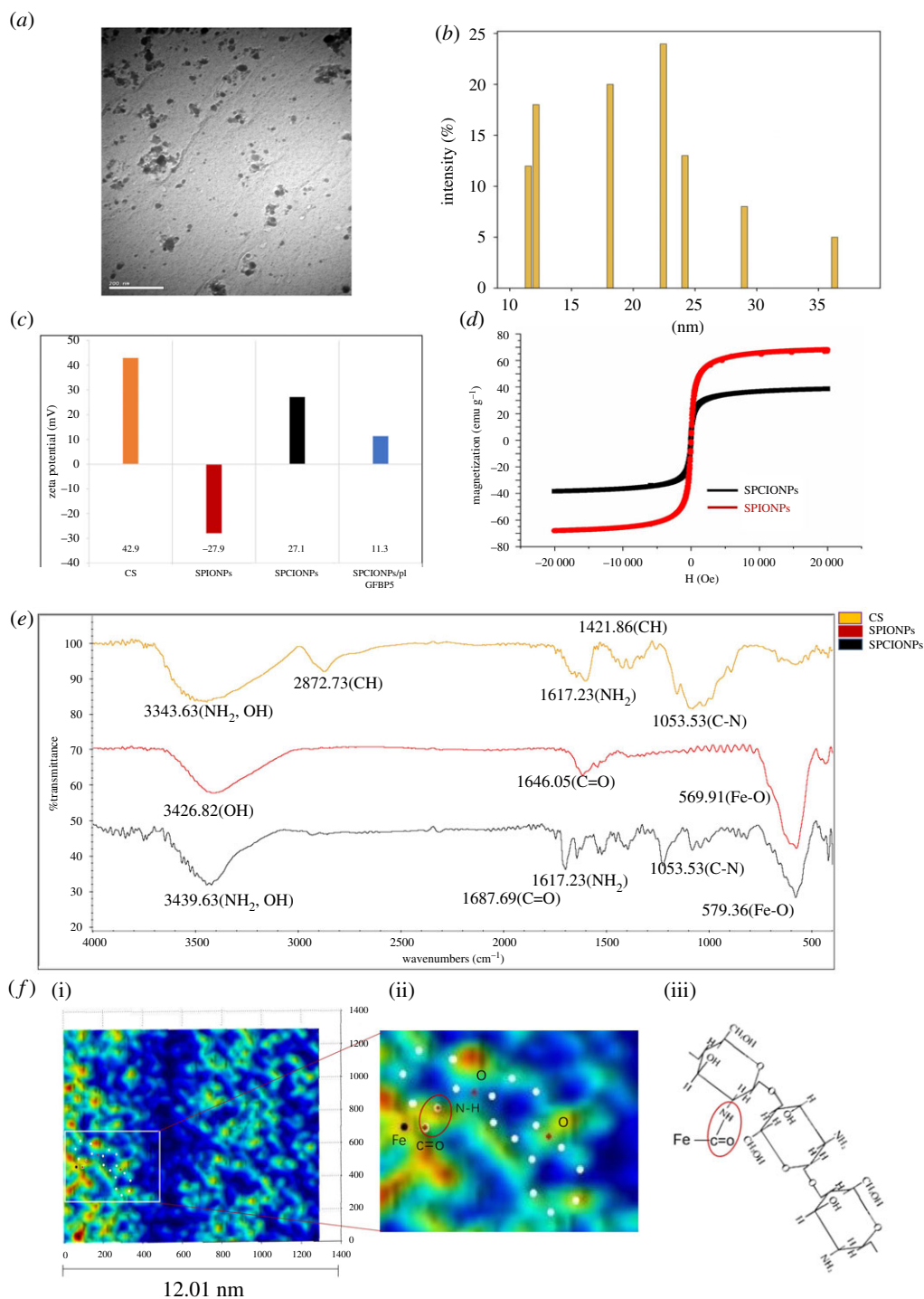


Figure 1. Characterization of SPIONPs and SPCIONPs. (a) TEM image of SPCIONPs; (b) the histogram to comment on size of SPCIONPs; (c) zeta potential of CS, SPIONPs, SPCIONPs and SPCIONPs/pIGFBP₅; (d) changes in magnetization curves of SPIONPs and SPCIONPs; (e) FT-IR spectra of CS, SPIONPs, and SPCIONPs; (f) (i) an AFM image; (ii) a partially enlarged image; (iii) molecular structure diagram.

fluorescence represented live cells. The number of red cells increased with time, and the number of red cells in the PEI/PUC19 group was the highest at the same time point.

3.5. Cell uptake assay and *in vitro* transfection

Figure 6 shows that FITC-CS/pIGFBP₅ and FITC-SPCIONPs/pIGFBP₅ were engulfed in endosomes, transported into the cells through endocytosis within 6 h after transfection and accumulated in large

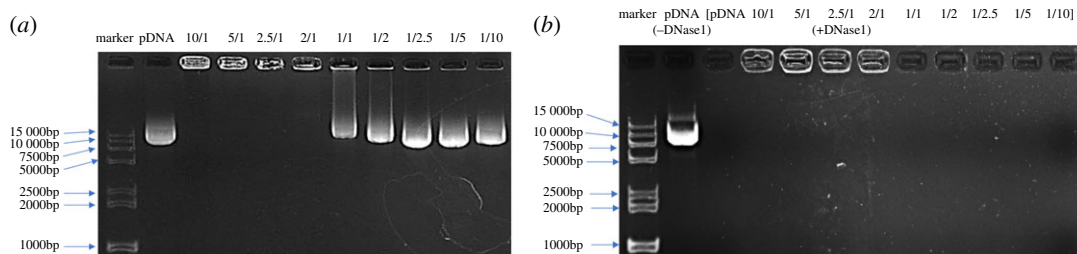


Figure 2. Agarose gel electrophoresis. (a) The combination of SPCIONPs and plasmids with different N/P ratios; (b) the combination of SPCIONPs and plasmids with different N/P ratios after DNase I addition.

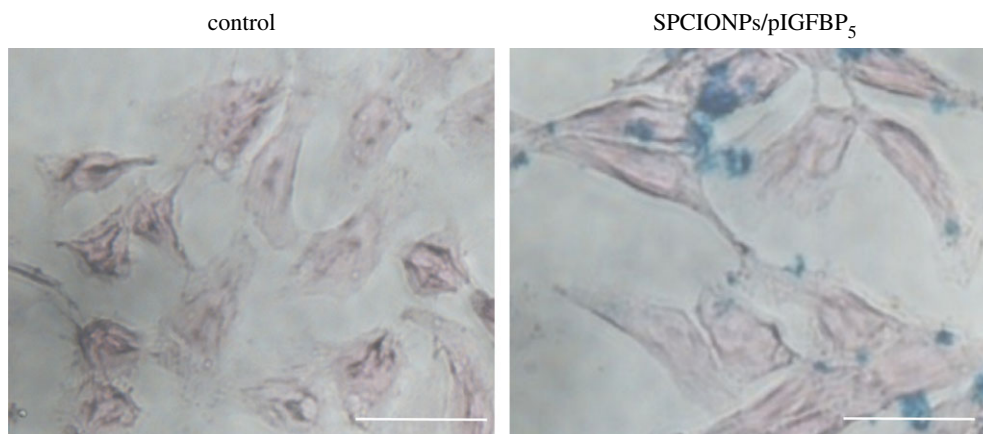


Figure 3. Prussian blue staining after transfection for 4 h. The scale bar is 100 μm .

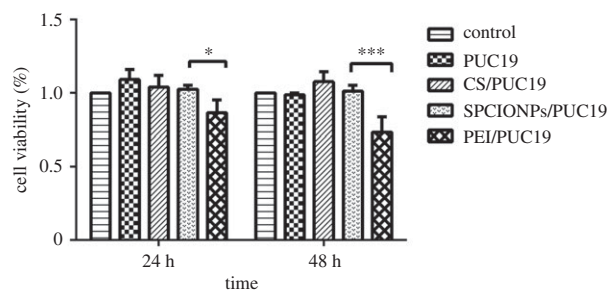


Figure 4. Cell survival was measured using a CCK8 assay. * $p < 0.05$; ** $p < 0.01$; *** $p < 0.001$.

quantities around the nucleus. The FITC-SPCIONPs/pIGFBP₅ group showed more green fluorescent particles around the nucleus. At 24 h, both groups had red fluorescence expression of the plasmids, while the red fluorescence expression in the FITC-SPCIONPs/pIGFBP₅ group was greater than that in the FITC-CS/pIGFBP₅ group.

As shown in figure 7, the red fluorescence expression in the PEI/pIGFBP₅ group (positive control group) was the highest of all groups. The red fluorescence expression in the SPCIONPs/pIGFBP₅ group at 24 h after transfection was more than that in the CS/pIGFBP₅ group, which was more than that in the control group. This result was consistent with the laser confocal microscopy result.

4. Discussion

In this study, SPCIONPs were prepared to load the IGFBP₅ plasmids, which could inhibit lung metastasis of osteosarcoma. The gene carrier was composed of carboxylated SPIONPs and CS. The surface of carboxylated modified SPIONPs was rich in carboxyl groups and can be recombined with amino-rich chitosan in the form of covalent bond. In many studies, chlorosulfonic acid supported piperidine-4-carboxylic acid (PPCA) [34], citric acid [27,28], PEG [35], oleic acid [36] and polyamide acid [37] were used to modify SPIONPs to make its surface touch carboxyl groups, which can be combined with

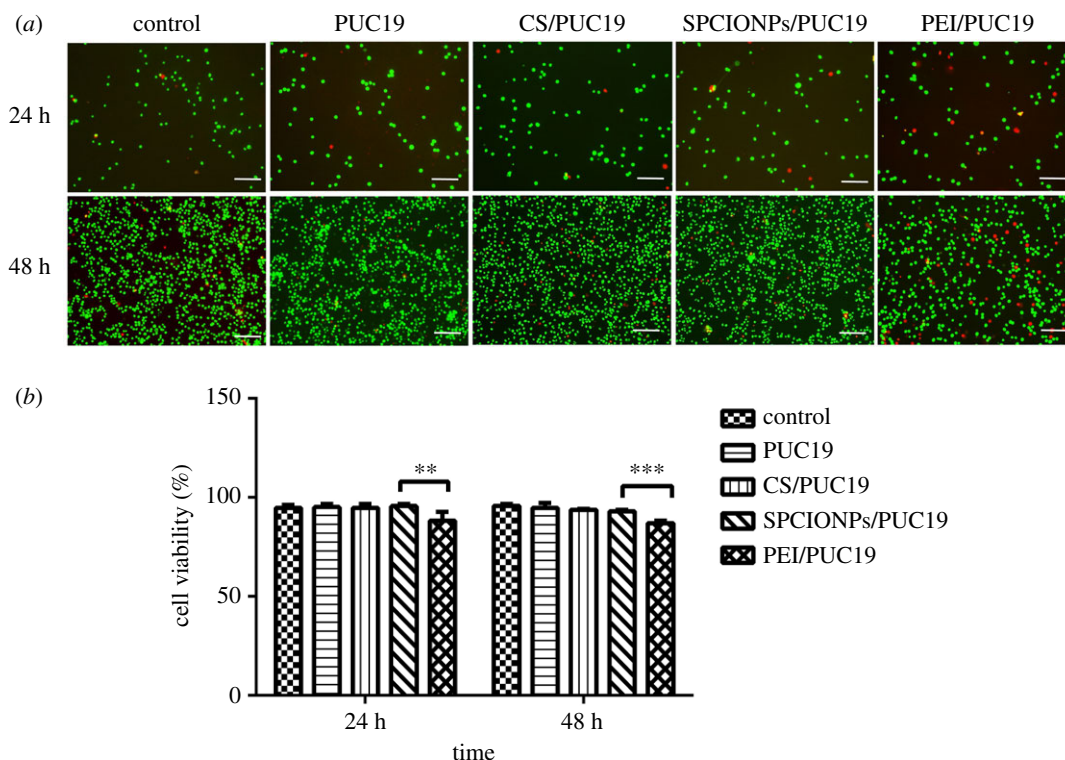


Figure 5. Cell survival was measured by a live–dead assay. (a) Red fluorescence represents dead cells, and green fluorescence represents live cells; (b) Quantitative analysis of cell viability. * $p < 0.05$; ** $p < 0.01$; *** $p < 0.001$; the scale bar is 100 μm .

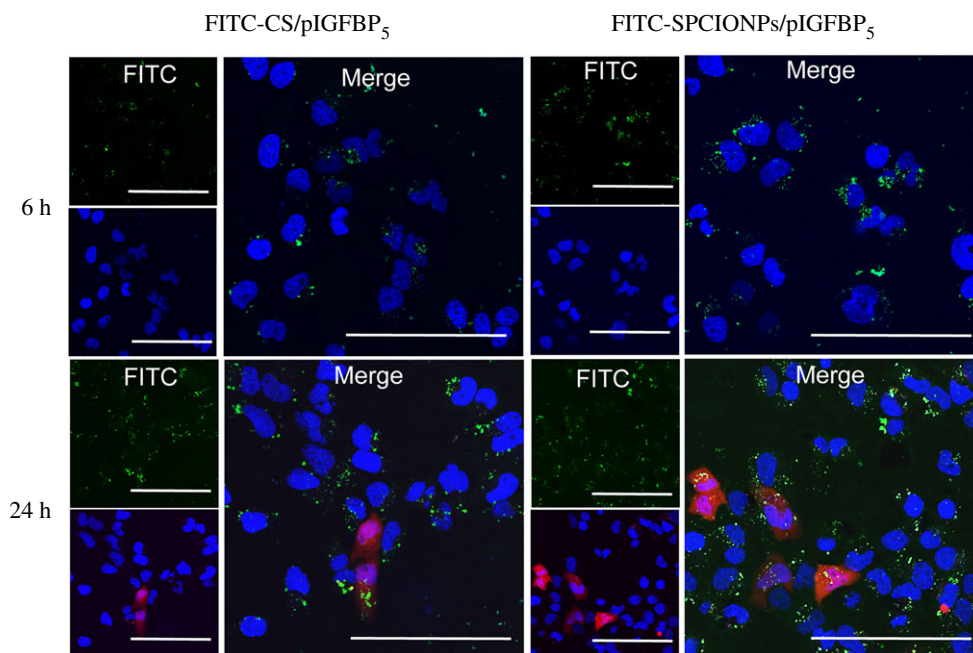


Figure 6. Nanoparticle complex uptake by cells after transfection for 6 and 24 h. Green fluorescence represents FITC-SPCIONPs/pIGFBP₅ and FITC-CS/pIGFBP₅, blue fluorescence indicates Hoechst-stained nucleus, and red fluorescence represents pIGFBP₅ expression. The scale bar is 100 μm .

different substances to show different functions. In our study, citric acid-modified SPIONPs were successfully prepared by chemical coprecipitation method. FTIR (figure 1e) showed that there were carboxyl absorption peaks and Fe–O absorption peaks on the surface of SPIONPs, indicating that we have successfully prepared citric acid modified superparamagnetic nanoparticles.

The carboxyl groups on the surface of SPIONPs and the amino groups of CS were connected by amide bonds through dehydration condensation. AFM and FTIR were used to detect the formation of

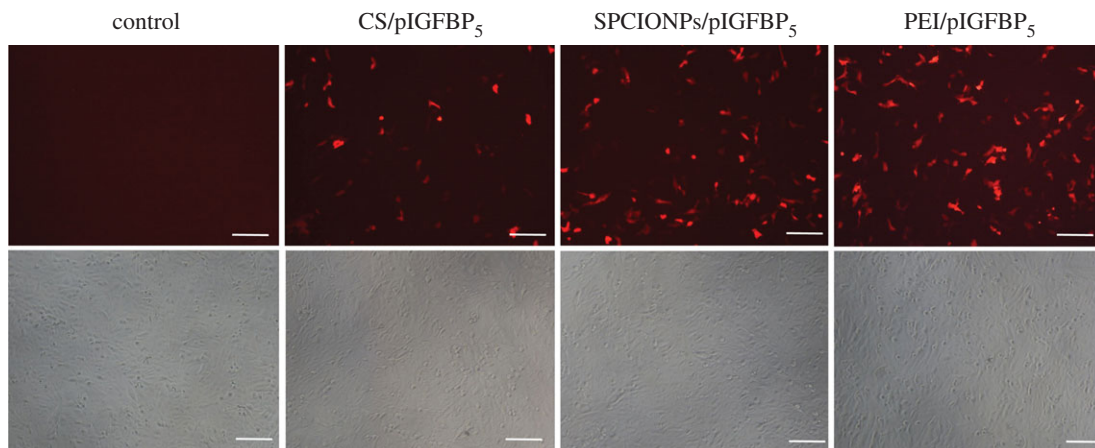


Figure 7. *In vitro* transfection of 143B cells. Transfection image under a fluorescence microscope at 100 \times magnification. The scale bar is 100 μ m.

amide bond (figure 1*e,f*). CS is a polycation due to its amino groups, which are ionized in weakly acidic environments, allowing the polymer to interact with negatively charged surfaces, such as cell membranes [38,39]. After CS was successfully grafted onto SPIONPs, they could bind a large number of concentrated plasmids and effectively protect them from DNA enzyme degradation (figure 2), which was one of the necessary conditions for cell transfection [40]. Because the zeta potential of SPCIONPs/pIGFBP₅ was 11.3 mV, the positively charged SPCIONPs/pIGFBP₅ easily bound to the negatively charged cell membrane (figure 3), as shown by Prussian blue staining, which was the initial condition of cell transfection [41].

The toxicity of gene vectors is an important parameter of gene release systems [38]. Reduced toxicity is a significant advantage of CS-modified carriers, and CS has been shown to have low toxicity in many *in vitro* experiments [33,42,43]. Unsoy *et al.* [29] showed that CS-encapsulated superparamagnetic iron oxide nanoparticles (CS-MNPs) had no obvious cytotoxicity to cells, and when CS-MNPs were applied at high doses (1000 μ g ml⁻¹) to HeLa cells, cell proliferation was reduced by only 2–5%. This observation is consistent with our research results. In this study, CCK8 and live–dead staining assays showed no significant difference between the SPCIONPs/pUC19 group and control group at 24 and 48 h (figures 4 and 5). Therefore, the SPCIONPs prepared in this study can serve as a non-viral vector with good biocompatibility and biosafety.

It is crucial to improve the transfection efficiency of CS as a gene vector system. CS is widely used in various fields due to its good biosafety. However, as a non-viral vector, chitosan does not have a strong proton-buffering effect, making it unable to escape from endosomes in a timely manner, leading to a lower transfection rate [40]. To increase the transfection rate of CS, Xu *et al.* [17] generated Arg-CS/pBMP-2 nanoparticles with arginine-linked CS to transfect preosteoblasts, Nam & Nah. [44] used CS-linked PEI to transfect colon cancer (HCT119) cells, and Wang *et al.* [45] prepared FA-PEG-CS to transfect liver cancer (HepG2) cells. However, magnetic transfection was used in this study, which forced the transfection vector and the target cell to stay in contact. In addition, the oscillation induced by magnetic transfection on the target cell surface can cause the nanoparticle complex to move, which helps increase the transfection rate by mechanically stimulating endocytosis [30,46,47]. Other researchers have shown that magnetic transfection can effectively increase the transfection rate of gene vectors [47,48]. Our *in vitro* transfection result showed that at 24 h, red fluorescence expression was greater in the SPCIONPs/pIGFBP₅ group than that in the CS/pIGFBP₅ group (figure 7). Laser confocal microscopy result showed (figure 6) that the FITC-SPCIONPs/pIGFBP₅ group exhibited greater red fluorescence expression with magnetic transfection because more nanoparticles accumulated around the nucleus. These findings confirm that magnetic transfection can promote transfection through targeted physical adsorption.

5. Conclusion

We successfully prepared carboxylated SPIONPs with a negative surface charge, which can combine with CS to form a non-viral vector called SPCIONPs. SPCIONPs have good biosafety, biocompatibility and can be tightly loaded with IGFBP₅ plasmids. Magnetic transfection can effectively promote

transfection of IGFBP₅ into 143B cells. Therefore, this magnetic transfection system has great potential in gene therapy for lung metastasis of osteosarcoma.

Data accessibility. Data available from the Dryad Digital Repository: <https://doi.org/10.5061/dryad.7m0cfxpr> [49].

Authors' contributions. Y.T. carried out the molecular laboratory work, participated in data analysis and drafted the manuscript; X.Q. and D.J. participated in the design of the study; J.W., Y.Z. and L.J. carried out the statistical analyses and critically revised the manuscript. All authors gave final approval for publication and agree to be held accountable for the work performed therein.

Competing interests. The authors declare no competing interests.

Funding. This work was supported by the medical research project of the Chongqing Science and Technology Commission (grant no. cstc2018jcyjAXO133) and Chongqing Municipal Health and Family Planning Commission (grant no. 2017MSXM048).

Acknowledgements. The authors thank Cong Luo from Children's Hospital of Chongqing Medical University for his great help in providing the laboratory for the preparation of superparamagnetic chitosan nanoparticles.

References

- Tang XF, Cao Y, Peng DB, Zhao GS, Zeng Y, Gao ZR, Lv YF, Guo QN. 2019 Overexpression of Notch3 is associated with metastasis and poor prognosis in osteosarcoma patients. *Cancer Manag. Res.* **11**, 547–559. (doi:10.2147/CMAR.5185495)
- Harrison DJ, Geller DS, Gill JD, Lewis VO, Gorlick R. 2018 Current and future therapeutic approaches for osteosarcoma. *Expert Rev. Anticancer Ther.* **18**, 39–50. (doi:10.1080/14737140.2018)
- Ferrari S, Serra M. 2015 An update on chemotherapy for osteosarcoma. *Expert Opin Pharmacother.* **16**, 2727–2736. (doi:10.1517/14656566.2015.1102226)
- Rikhof B, deJong S, Suurmeijer AJ, Meijer C, van der Graaf WT. 2009 The insulin-like growth factor system and sarcomas. *J. Pathol.* **217**, 469–482. (doi:10.1002/path.2499)
- Luther GA *et al.* 2013 IGFBP₅ domains exert distinct inhibitory effects on the tumorigenicity and metastasis of human osteosarcoma. *Cancer Lett.* **336**, 222–230. (doi:10.1016/j.canlet.2013.05.002)
- Su Y *et al.* 2009 Establishment and characterization of a new highly metastatic human osteosarcoma cell line. *Clin. Exp. Metastasi.* **26**, 599–610. (doi:10.1007/s10585-009-9259-6)
- Pan D, Büning H, Ling C. 2019 Rational design of gene therapy vectors. *Mol. Ther. Methods Clin. Dev.* **12**, 246–247. (doi:10.1016/j.omtm.2019.01.009)
- Mansouri S, Lavigne P, Corsi K, Benderdour M, Beaumont E, Fernandes JC. 2004 Chitosan-DNA nanoparticles as non-viral vectors in gene therapy: strategies to improve transfection efficacy. *Eur. J. Pharm. Biopharm.* **57**, 1–8. (doi:10.1016/s0939-6411(03)00155-3)
- Cao Y, Tan YF, Wong YS, Liew MWJ, Venkatraman S. 2019 Recent advances in chitosan-based carriers for gene delivery. *Mar. Drugs* **17**, 381. (doi:10.3390/md17060381)
- Namgung R, Singha K, Yu MK, Jon S, Kim YS, Ahn Y, Park IK, Kim WJ. 2010 Hybrid superparamagnetic iron oxide nanoparticle-branched polyethylenimine magnetoplexes for gene transfection of vascular endothelial cells. *Biomaterials* **31**, 4204–4213. (doi:10.1016/j.biomaterials)
- Wang J, Dou B, Bao Y. 2014 Efficient targeted pDNA/siRNA delivery with folate-low molecular weight polyethylenimine-modified pullulan as non-viral carrier. *Mater. Sci. Eng. C Mater. Biol. Appl.* **34**, 98–109. (doi:10.1016/j.msec.2013.08.035)
- Shen J, Zhao DJ, Li W, Hu QL, Wang QW, Xu FJ, Tang GP. 2013 A polyethylenimine-mimetic biodegradable polycation gene vector and the effect of amine composition in transfection efficiency. *Biomaterials* **34**, 4520–4531. (doi:10.1016/j.biomaterials.2013.02.068)
- Mobarakeh VI, Modarressi MH, Rahimi P, Bolhassani A, Arefian E, Atyabi F, Vahabpour R. 2019 Optimization of chitosan nanoparticles as an anti-HIV siRNA delivery vehicle. *Int. J. Biol. Macromol.* **129**, 305–315. (doi:10.1016/j.ijbiomac.2019.02.036)
- Casadidio C, Peregrina DV, Gigliobianco MR, Deng S, Censi R, DiMartino P. 2019 Chitin and chitosans: characteristics, eco-friendly processes, and applications in cosmetic science. *Mar. Drugs* **17**, 369. (doi:10.3390/md17060369)
- Garg U, Chauhan S, Nagaich U, Jain N. 2019 Current advances in chitosan nanoparticles based drug delivery and targeting. *Adv. Pharm. Bull.* **9**, 195–204. (doi:10.15171/apb.2019.023)
- Wang CX *et al.* 2019 Superparamagnetic chitosan nanoparticles for a vancomycin delivery system: optimized fabrication and in vitro characterization. *J. Biomed. Nanotechnol.* **15**, 2121–2129. (doi:10.1166/jbn.2019.2831)
- Xu X, Qiu S, Zhang Y, Yin J, Min S. 2017 PELA microspheres with encapsulated arginine-chitosan/pBMP-2 nanoparticles induce pBMP-2 controlled-release, transfected osteoblastic progenitor cells, and promoted osteogenic differentiation. *Artif. Cells Nanomed. Biotechnol.* **45**, 330–339. (doi:10.3109/21691401.2016.1153480)
- Manatunga DC, deSilva RM, deSilva KMN, deSilva N, Bhandari S, Yap YK, Costha NP. 2017 pH responsive controlled release of anticancer hydrophobic drugs from sodiumalginate and hydroxyapatite bicoated iron oxide nanoparticles. *Eur. J. Pharm. Biopharm.* **117**, 29–38. (doi:10.1016/j.ejpb.2017.03.014)
- Manatunga DC, de Silva RM, de Silva KMN, Malavige GN, Wijeratte DT, Williams GR. 2018 Effective delivery of hydrophobic drugs to breast and liver cancer cells using a hybrid inorganic nanocarrier: a detailed investigation using cytotoxicity assays, fluorescence imaging and flow cytometry. *Eur. J. Pharm. Biopharm.* **128**, 18–26. (doi:10.1016/j.ejpb.2018.04)
- Manatunga DC, de Silva RM, de Silva KMN, Wijeratte DT, Malavige GN, Williams G. 2018 Fabrication of 6-gingerol, doxorubicin and alginate hydroxyapatite into a bio-compatible formulation: enhanced anti-proliferative effect on breast and liver cancer cells. *Chem. Cent. J.* **12**, 119. (doi:10.1186/s13065-018-0482-6)
- Manatunga DC, Godakanda VU, de Silva RM, de Silva KMN. 2019 Recent developments in the use of organic-inorganic nanohybrids for drug delivery. *Wiley Interdiscip. Rev. Nanomed. Nanobiotechnol.* **12**, e1605. (doi:10.1002/wnan.1605)
- Duan J *et al.* 2019 Iron oxide nanoparticles promote vascular endothelial cells survival from oxidative stress by enhancement of autophagy. *Regen. Biomater.* **6**, 221–229. (doi:10.1093/rb/rbz024)
- Tamsir NM, Esa NM, Shafie NH, Hussein MZ, Hamzah H, Abdullah MA. 2019 The acute effects of oral administration of phytic acid-chitosan-magnetic iron oxide nanoparticles in mice. *Int. J. Mol. Sci.* **20**, 4114. (doi:10.3390/ijms20174114)
- Dadfar SM, Roemhild K, Drude NI, vonStillfried S, Knüchel R, Kiessling F, Lammers T. 2019 Iron oxide nanoparticles: diagnostic, therapeutic and theranostic applications. *Adv. Drug Deliv. Rev.* **138**, 302–325. (doi:10.1016/j.addr.2019.01.005)
- Britos TN, Castro CE, Bertassoli BM, Petri G, Fonseca FLA, Ferreira FF, Haddad PS. 2019 In vivo evaluation of thiol-functionalized superparamagnetic iron oxide nanoparticles. *Mater. Sci. Eng. C Mater. Biol. Appl.* **99**, 171–179. (doi:10.1016/j.msec.2019.01.118)
- Wu W, He Q, Jiang C. 2008 Magnetic iron oxide nanoparticles: synthesis and surface

- functionalization strategies. *Nanoscale Res. Lett.* **3**, 397–415. (doi:10.1007/s11671-008-9174-9)
27. Antic B, Boskovic M, Nikodinovic-Runic J, Ming Y, Zhang H, Bozin ES, Janković D, Spasojevic V, Vranjes-Djuric S. 2017 Complementary approaches for the evaluation of biocompatibility of ^{90}Y -labeled superparamagnetic citric acid (Fe_3O_4) coated nanoparticles. *Mater. Sci. Eng. C Mater. Biol. Appl.* **1**, 157–164. (doi:10.1016/j.msec.2017.02.023)
 28. Patel U, Chauhan K, Gupte S. 2018 Synthesis, characterization and application of lipase-conjugated citric acid-coated magnetic nanoparticles for ester synthesis using waste frying oil. *J. Biotech.* **8**, 211. (doi:10.1007/s13205-018-1228-9)
 29. Unsoy G, Yalcin S, Khodadust R, Gunduz G, Gunduz U. 2012 Synthesis optimization and characterization of chitosan-coated iron oxide nanoparticles produced for biomedical applications. *J. Nanopart. Res.* **14**, 964. (doi:10.1007/s11051-012-0964-8)
 30. Cen C *et al.* 2019 Improving magnetofection of magnetic polyethylenimine nanoparticles into MG-63 osteoblasts using a novel uniform magnetic field. *Nanoscale Res. Lett.* **14**, 90. (doi:10.1186/s11671-019-2882-5)
 31. Chen D, Gan H, Huang X, Shen Q, Du X, Tang W, Yang X. 2012 Effects of peripheral blood mononuclear cells morphology on vascular calcification in uremic patients on maintenance hemodialysis. *Ther. Apher. Dial.* **16**, 173–180. (doi:10.1111/j.1744-9987.2011.01044)
 32. Li B, Wen M, Li W, He M, Yang X, Li S. 2011 Preparation and characterization of baicalin-poly-vinylpyrrolidone coprecipitate. *Int. J. Pharm.* **15**, 91–96. (doi:10.1016/j.ijpharm.2011.01.055)
 33. Barahue F, Dorniani D, Saifullah B, Gothai S, Hussein MZ, Pandurangan AK, Arulselvan P, Norhaizan ME. 2017 Sustained release of anticancer agent phytic acid from its chitosan-coated magnetic nanoparticles for drug-delivery system. *Int. J. Nanomedicine.* **12**, 2361–2372. (doi:10.2147/IJN.S126245)
 34. Habibzadeh S, Ghasemnejad-Bosra H, Haghdad M, Heydari-Parastar S. 2019 Chlorosulfonic acid supported piperidine-4-carboxylic acid (PPCA) functionalized Fe_3O_4 nanoparticles (Fe_3O_4 -PPCA): the efficient, green and reusable nanocatalyst for the synthesis of pyrazolyl coumarin derivatives under solvent-free conditions. *Comb. Chem. High Throughput Screen* **22**, 123–128. (doi:10.2174/1386207322666190325120715)
 35. Barick KC, Sharma A, Shetake NG, Ningthoujam RS, Vatsa RK, Babu PD, Pandey BN, Hassan PA. 2015 Covalent bridging of surface functionalized Fe_3O_4 and YPO_4 :Eu nanostructures for simultaneous imaging and therapy. *Dalton Trans.* **44**, 14686. (doi:10.1039/c5dt01522g)
 36. Wu C, Xu C, Ni H, Yang Q, Cai H, Xiao A. 2016 Preparation and characterization of tannase immobilized onto carboxyl-functionalized superparamagnetic ferroferric oxide nanoparticles. *Bioresour. Technol.* **205**, 67–74. (doi:10.1016/j.biortech.2016.01.032)
 37. Miao C, Hu F, Rui Y, Duan Y, Gu H. 2019 A T/T dual functional iron oxide MRI contrast agent with super stability and low hypersensitivity. *J. Biomed. Mater. Res. B Appl. Biomater.* **28**, 2081–2091. (doi:10.1039/c9tb00002j)
 38. Wang F, Pang JD, Huang LL, Wang R, Li D, Sun K, Wang LT, Zhang LM. 2019 Nanoscale polysaccharide derivative as an AEG-1 siRNA carrier for effective osteosarcoma therapy. *Int. J. Nanomedicine.* **13**, 857–875. (doi:10.2147/IJN.S147747)
 39. Zhao LM, Shi LE, Zhang ZL, Chen JM, Shi DD, Yang J, Tang ZX. 2011 Preparation and application of chitosan nanoparticles and nanofibers. *Braz. J. Chem. Eng.* **28**, 353–362. (doi:10.1590/S0104-66322011000300001)
 40. Zhao QQ, Chen JL, Lv TF, He CX, Tang GP, Liang WQ, Tabata Y, Gao JQ. 2009 N/P ratio significantly influences the transfection efficiency and cytotoxicity of a polyethylenimine/chitosan/DNA complex. *Biol. Pharm. Bull.* **32**, 706–710. (doi:10.1248/bpb.32.706)
 41. Sosa Acosta JR, Iriarte Mesa C, Ortega GA, Díaz-García AM. 2020 DNA-iron oxide nanoparticles conjugates: functional magnetic nanoplatforms in biomedical applications. *Top. Curr. Chem.* (Cham.) **378**, 13. (doi:10.1007/s41061-019-0277-9)
 42. Malakooty Poor E, Baghaban Eslaminejad M, Gheibi N, Bagheri F, Atyabi F. 2014 Chitosan-pDNA nanoparticle characteristics determine the transfection efficacy of gene delivery to human mesenchymal stem cells. *Artif. Cells Nanomed. Biotechnol.* **42**, 376–384. (doi:10.3109/21691401.2013.832685)
 43. Corsi K, Chellat F, Yahia L, Fernandes JC. 2003 Mesenchymal stem cells, MG63 and HEK293 transfection using chitosan-DNA nanoparticles. *Biomaterials* **24**, 1255–1264. (doi:10.1016/s0142-9612(02)00507-0)
 44. Nam JP, Nah JW. 2016 Target gene delivery from targeting ligand conjugated chitosan-PEI copolymer for cancer therapy. *Carbohydr. Polym.* **135**, 153–161. (doi:10.1016/j.carbpol.2015.08.053)
 45. Wang M *et al.* 2013 A pH-sensitive gene delivery system based on folic acid-PEG-chitosan – PAMAM-plasmid DNA complexes for cancer cell targeting. *Biomaterials* **34**, 1012010132. (doi:10.1016/j.biomaterials.2013.09.006)
 46. Vernon MM, Dean DA, Dobson J. 2015 DNA targeting sequence improves magnetic nanoparticle-based plasmid DNA transfection efficiency in model neurons. *Int. J. Mol. Sci.* **16**, 19 369–19 386. (doi:10.3390/ijms160819369)
 47. Fouriki A, Clements MA, Farrow N, Dobson J. 2014 Efficient transfection of MG-63 osteoblasts using magnetic nanoparticles and oscillating magnetic fields. *J. Tissue Eng. Regen. Med.* **8**, 169–175. (doi:10.1002/term.1508)
 48. Yamoah MA *et al.* 2018 Highly efficient transfection of human induced pluripotent stem cells using magnetic nanoparticles. *Int. J. Nanomedicine.* **13**, 6073–6078. (doi:10.2147/IJN.S172254)
 49. Tang Y, Wu J, Zhang Y, Ju LP, Qu XY, Jiang DM. 2020 Data from: Magnetic transfection with superparamagnetic chitosan-loaded IGFBP5 nanoparticles and their in vitro biosafety. Dryad Digital Repository. (doi:10.5061/dryad.7m0cfxpr)